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# Importance of Polyvinylpyrrolidon as Pyrrolidone-Based Surfactants and as Poly (*N*-vinylpyrrolidone)-Modified Surfaces for Biomedical Applications. A Review

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#### Abstract

The common name of N-vinyl-2-pyrrolidone (NVP), watersoluble homopolymer, is Polyvinyl pyrrolidone (PVP, povidone), which is also named PVP in this study. The common name of the NVP crosslinked insoluble homopolymer (PPVP, crospovisone) is polyvinylpolypyrrolidone. The surface-active properties of the alkyl group of N-alkylated pyrrolidones expand to C8P. The resulting surfactant will interact with the iron surfactant synergistically. A useful alternative is pyrrolidone. This can improve the efficiency by increasing water solubility and compatibilities of different tensile structures. Moreover, in combination with derivatives the pyrrolidone ring usually reduces toxicity. The simple water soluble synthetic polymer (PVP) with many beneficial properties such as low toxicity, chemical stability and high biocompatibility. Poly (N vinylpyrrolidone) (PVP). Because PVP is inert and hem compatible, it has been used as a blood substitute for plasma. In recent years, PVP has extensively studied surface modulation to prevent unspecific protein adsorption. This means that PVP can be used as an effective poly-ethylene glycol (PEG) surface alternator. This study reveals a quick analysis and use of PVP together with shampoo

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and agricultural formulations and the use of PVP and its co-polymers as well as possible biomedical (BM) application of PM materials.

**Keywords:** Polyvinylpyrrolidon; Pyrrolidone-Based Surfactants; Poly (N-vinylpyrrolidone); Biomedical Applications; Modified Materials

# 1. INTRODUCTION

The generic name for the water-soluble N-vinyl-2-pyrrolidone homopolymer (NVP) is Polyvinylpyrrolidon (PVP), which is simply called PVP. The common name of NVP's interlinked, insoluble homopolymer is polyvinyl polypyrrolidone (PVPP, crospovidone) [1]. First in Germany founded at l. G. In the 1930s, PVP is commonly used as an Alternative Blood Plasma and Extender during World War II, as a color by Professor Walter Reppe and his associates. This is upside as non-antigenic, allowing no cross mixing and avoiding the chances of blood-related infectious diseases. It was supplemented by other products in later years. The problem of productivity in the parenteral administration of 3.5 percent PVP (K-30), though, was also part of the US. Implementation of the Drug Effectiveness Test (DESI) review program and recorded to be effective in correcting low blood volumes in shock treatment [1, 2].

A great number of other applications are now included in PVP. The market success comes from its biological viability, low toxicity, film forming and adhesive properties, unique complexing ability, relative sluggishness to salts and acids and thermal resistance to solution degradation. PVP has major applications for many sectors, particularly pharmacy, foodstuffs, beverages, cosmetics, toiletries and the photography industry, because of these distinct characteristics [1, 3]. In view of the existence of PVP, homopolymers, copolymers and crosslinking PVP are accessible in three different forms.

In the light of its hydrophilicity [4], PVP contributed to water solubility of derivatives, which gradually led to 2 financially important products: polyvinylpyrrolidone, ultra-low inflammation complexing polymer [6] and C-methylpyrrolidone (C1P) [6].

In addition, the surface-active features of C8P that become essential for N-alkyl group pyrrolidones. This reaction may be correlated with an anionic surface agent synergistically. The association is driven by a carbonyl oxygen electron-negative pyrrolidone, which can cause a proton to form a quaternary pseudo ammonium ion that can form a pair of anions with big anions. The hydrophobic relations between the two alkyl chains are also balanced. However, pyrrolydone can associate electrostatically with aromatics, nonionic Polyvinylpyrrolidon hydrogen bonding, and hydrophobic activity. This partnership will turn the functional pyrrolidone group from one hydrophobic traction shape into another. It's an efficient substitute for pyrrolidone. This may improve the performance and flexibility of various tensile frameworks. In fact, in conjunction with compounds, the pyrrolidone ring typically reduces toxicity [7].

As a result, the "PVP," a crucial water-soluble polymer synthesized for the first time around 70 years prior to the use of acetylene chemistry, is poly (N-vinylpyrrolidone) [8, 9]. Nvinylpyrrolidone polymerization is a polymer medicine. A polymerized volume, water or even suspension is possible with N-vinylpyrrolidone. The PVP, with molecular masses from 2500 Da to nearly 1 million Da, is mainly accomplished with the application of radical polymerization in solution [10]. PVP may be soluble in polar solvents like water and in some non-polar organic solvents like dichloromethane, butanol, and chloroform [11]. Their solutions are essential.

The hydrophilicity of the polar-lactam group in the pyrrolidone process increases due to the water solubility of PVP. PVP's lipophilic character is attributed to non-polar groupings of methylene. The brilliant solubility of traditional PVP solvents led to its wide pharmaceutical use in almost entire dosage forms. For instance, the development of tablets, wet granulation, injectile and topical solutions, oral solutions, syrups, drops and film coatings on tablets [12]. Thanks to the characteristics of film making, PVPs are used in transdermal systems, medicinal spray and screen-covering of tablets.

Because of its chemical composition, PVP creates complexes with other low molecular mass substances as well as various polymers. It is usually desirable to be able to generate complexes because insoluble substances may be solubilized [13]. The ability to produce a complex is

especially important because of PVP-iodine (povidone iodine). Many of these complex formulations were used in antibiotic soaps, operative hand scrubs, pre-operative patient skin injury cleansers [1,2] and low hazard and high-capacity herbicides [1,15].

### 2. APPLICATION OF PVP

In foodstuffs, cosmetics, textiles and adhesives PVP is commonly used. The WHO Joint Expert Committee on Food Additives (JECFA) has granted an Acceptable Daily Intake (ADI) of 0-50 mg/kg/day for PVP (WHO, 1986) Under United States Law, PVP has a number of permitted uses in foodstuffs, including use as a binder for vitamin and mineral concentrate tablets. Cattle tints and dressings for skin cleaning and preventive treatments and hair tints may be mixed with PVP and other creams can be made with PVP either gray or nonsense [16] PVP. It serves as a replacement of hair lotions and increases shampoo quality and home-based detergents to preserve the scalp. PVP has been used for other polyphenolic substances such as beer and wine anthocyanogenes because of their capacity to complex and shape insoluble precipitates, to be replaced for insoluble PVPP in this submission. It is also used for food colors as a dilatant and dispersant.

Table 1: Viscosity Response	(peak viscosities with	N-dodecylpyrrolidone)
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Anionic $(12\% \text{ actives})^a$	Peak viscosity (CPS)	Nonionic level (%)
TEALS	18 K	6.0
AOS	36 K	6.0
SLS	$25~{ m K}$	5.0
SLES (3 mole)	61 K	5.5
ALS	78 K	2.5

<sup>a</sup>TEALS, triethanolamine lauryl sulphate; SLES, sodium laureth sulphate; SLS, sodium lauryl sulphate; AOS, α-olefin sulphonate, and ALS, ammonium lauryl sulphate. <sup>b</sup>Brookfield RVT Viscometer, Helipath Stand, T-C Spindle at 10 rpm for 1 min at 25°C.

The pyrrolidones C12 and C8 are marginally solutions of water but consume 20 to 35% of water if the surfactants are strong (Figure 1). Conversely, in specific polar solvents or in water (Table 2), they are soluble and may generate reverse micelles. In fact, they are able to

combine hydrogen bonding with active polar locations, which can be used in agricultural concentrate formulations [7].



Figure. 1. Aqueous solubility of pyrrolidones.

Table 2: Solubility of N-Alkyl Pyrrolidones (10% w/w at 25 °C) a

Solvent	C8/C12	N-Cocoamidoethyl
pyrrolidone		
Acetone	S	S
Ethanol	S	S
Xylene	S	DS
Heptane	S	IS
Paraffin oil	S	IS
Stoddard solvent	S	IS
Perchloroethylene	S	S

<sup>a</sup>S, soluble; IS, insoluble; and DS, dispersible.

The synthesis of hydro fluoride macromolecules in the skin will affect the biological availability of ingredients. The most widely used polymers are PEG, polyethylene glycol and its components [18]. Polysaccharides, polyamides, and polyurethane related polybutane and polyfamulites are also used. The main impact of these converters is, for example, reducing intracellular biofuels by reducing protein synthesis and proliferation. The degree of antibiotics in PVP has also increased in momentum over the last few days. The fibrinogen gravity has been converted to PVP and is not classified as PEG [19]. PVP should also be viewed as an efficient PEG anti-inflammatory. Many changes in PVP for biomedicine have been made. The efficiency of the procedure, for example, is designed to improve the blood properties of central polyurethane venous catheters, natural life. Several approaches are

actually being used to build mechanisms to counter fraud. It is successful in conjunction with PVP against biopharmaceutical tablets. Aerodynamic molecules (SPRs, for instance) have been updated by PVP and biosensors and biochips have been demonstrated [20].

### 3. THE USE OF SURFACE CHANGE PVP

#### 3.1 Physical Coating

Clear and effective surface modulation system used for the control of PVP surfaces is physical coating. Polyurethane catheters have been found to be mildly hydrophilic ally coated with PVP and to have fibrogen and fibronectin (FN) levels considerably lower than non-coated catheters. A significant drop in protein-mediated adherence to Staphylococcus aureus and Staphylococcus epidermis has resulted in poor protein absorption [21].

The key problem is that the foundation is weakly attached to the lamination surface [22]. Usually, coating techniques struggle due to limited repeats.

#### 3.2 Modification via Blending

PP (polypropylene), PAN (polyacrylonitrile), PSF (polysulfide), and PVSP (polyvinyl fluoride) are also evident among the synthetic polymers used for biomedical membrane material. However, the use of these components could be encountered in situations such as protein denaturation and blood coagulation induced by protein fouling [23]. Mixing alteration is used to overcome these problems by combining hydrophilic polymers.

Past studies have shown the impact on biocompatibility of the molecular mass of PVP. For example, in human beings antigenic is PVP with a large molecular weight (K-87, MW = 1000, 0000D), while in human beings antigenic (60, 61) is not antifungal with little molecular weight (10,000 - 40,000D) [24]. PVPs of different molecular masses were used in membrane spinning as hydrophilizing additives [25]. At the 10 wt. per cent PVP, empty MM = 360 kDa PVP fiber filters were the most hydrophilic and the best hair filtration preservation function and anti-fouling features have been demonstrated. The mixing change provides high repeatability and control parameters. Therefore, the

adjustment in the composition of the mixture can be extended for components that maintain their mechanical characteristics with increased biocompatibility. For example, PVP/PSF-based film PVPs of 1-5 Wt. percent are the lowest platelet connection and adsorption of the PVP (1200 000 Da) molecular mass in blood touch experiments. The materials together, for example, provided outstanding mechanical durability.



Figure 2. Swelling/shrinking behavior of polymer particles on APS-150E.

Although the biocompatibility of PVD is greatly improved and the mixing process is often artless, the PVP loss from diversified substances in interaction with tissues and blood is a most important enduring concern. A specific method of PVP aggregation is the application of various monomers NVP copolymers [26]. A new amphiphilic triblockcopolymer form Poly (N-vinylpyrrolidone)-b-polyethylmethacrylate)-bpolyethyl-(N-vinyl-polyrrolidone) (PVP-b-PMMA-b-PVP) was formed in the process of reversible attachment fragmentation chain transfer polymerization. The PES will combine these copolymers to manufacture hollow and smooth fiber membranes. The polymer (brush) blocks of PMMA developed on the face of the membrane while the block of PMMA was closely linked to PES which provided an unchanged hydrophilicity of the membrane and simultaneously prevented the liquidation of PVP. Such biocompatible membranes provide important advantages in terms of blood separation [27].

# 3.3 Photochemical NVP Grafting

Ultraviolet (UV) radiation is frequently used for photochemical grafting. The grafting technique can be restricted to the surface /

surface, since the transmission of UV is typically small, thus not affecting the bulk properties of parts. Numerous reports of NVP photochemical grafting changed polymer surfaces are visible. Next, UV graft polymerization by 3-hydrophilic monomers, NVPs, Nvinylformamides, and N-vinylcaprolactams has achieved PES ultrafiltration membrane modification [28]. With half a drop in BSA adsorption and 4% more maintenance than the unmodified PES membrane, the NVP-grafted membrane was the best performance. The reverse micro emulsion of methylenebisacrylamide was adjusted with PP and poly (ethylene terephthalate) (PET) by means of NVP / N UV induced grafting [12]. On the graft materials the point of contact of water was seen below 50 (stable over time). At the same time, polymer clarity was not compromised by surface change.

The nature of the UV processes for complicated structures such as the internal surface of tubular materials is one of the main limitations.

# 3.4 Application of radiation and NVP

The ionizing radiation system forms a solid surface on the surface of the material, which allows polymerization. There are many refined substances. including rubber. poly (L-lactide), poly (hexafluoropropylene fluoride), polyethylene (PE) and PP [30]. It is shown to enhance the image and polymerization of UV active, embedded in PP membrane. It has been observed that ray-induced implantation causes a significant reduction in draft rate. The effects of air contact are minimized by correction. The absorption of BSA and the cost of the installed PVP layer, therefore, significantly decreased compared to the controls. UV damage was detrimental as waves below 280 nm resulted in small starting points as a result of solar radiation and NVP monomer [31], due to low exposure [31], although most of the benefits of electricity can be used, the main disadvantage of matter is the unavailability of material properties.

# 3.5 plasma polymers NVP

The application of polymerized plasma for grafting is limited to the surface of polymeric material and therefore, it has little effect on bulk characteristics, relative to grafting by  $\beta$ -radiation-induced.

Polymerization of grafting of various particles by plasma was one of the best common surface alteration strategies used in recent years [32]. NVP plasma polymerization on several substrates has been largely performed. For starters, plasma polymerization. For starters. The complementary activation decrease of PVP grafted Silicone was 90 percent lower than non-treated Silicone. Further analysis contributed to the assumption that condensed supplemental PVP-grafted surface activities resulted from either low general or low C3-binding protein adsorption, with certain alterations in the composition of protein layers. Other findings that establish a causal link between general protein adsorption and complementary activation are contrary.

### **3.6 Surfaces of PVP-Chemical alteration**

The substratum surface needs connection of the polymer chains covalently for chemical modification. The surface bonding of polymers is usually stable and durable surfaces are obtained. Polymer chains linked to covalence can be rendered by "grafting" or by "grafting" [33]. The method of "grafting to" involves chemical reaction to attach a preformed, functionalized polymer to the surface. A 4-[4'-azidobenzoy]]oxo-n-butyl methacrylate group of copolymers and aryl azide was developed. A highly reactive electrophilic mid-section formed by the aryl azide segment was processed with poly (urethane) urethane surface group. This film was less chromogenous than polyurethane that was not modified [34].

Actually, the "grafting to" approach has many restrictions. A steric repulsion between grafted polymer chains, for example, will inhibit the production of high MW and grafted polymer brushes. At the other side, even though an extremely large molecular weights are obtained in grafting processes the duration and sterically the chain of MW of graft is not inhibited. Sterically the density at the surface of the originator is uncontrolled because the originator is a tiny molecule. Classic free polymerization, RAFT polymerization methods etc. [35] can be used on substratum surfaces for chemical grafting — PVP can be used for this reason.

Radical NVP polymerization on several substrates has been a big research challenge. PVP-grafted PSF membranes on vinylfunctional surfaces by NVP polymerization. The shifting surfaces

demonstrated increased protein adsorption and significantly less plasma adhesion than controls [15] develops CS-graft- PVP surfaces. To degrade the water touch angles which demonstrated the addition of a hydrophilic surface to the blending of radical graft polymerizations. The protein amount adsorbed by the three-surface was also reduced in the same amount, and the CS-greffee-PVP adsorption by BSA was far lower compared to the CS and PVP combination.

#### 4. CONCLUSION

PVP finds ways to expand biomedical applications as a synthetic polymer with a rare combination of water soluble characteristics, stability of structure, general bio-inertness and bio-compatibility and. In addition, the PVP layer is easily isolated by simple covering techniques, thereby making these solutions inaccessible to long distance applications. Monomer absorption at wavelengths below 280 nm is prevented in UV-initiated polymerization procedures which trigger poor degrees of grafting. While the use of u-radiation for initiation can achieve high degrees of grafting, the loss of mechanical properties in this procedure is inacceptable. The PVP rings can be broken with the subsequent biocompatibility degradation using plasma polymerization techniques. These issues are prevented by chemical grafting and seen as a successful surface alteration medium using PVP. One of the successful methods for chemical alteration is ATRP. The polymerization of a non-conjugated monomer such as NVP by using ATRP is very difficult. A highly competent catalyst system can require distinct polymerization of ATRP on material surfaces. The excellent protein tolerance of PVP-modified surfaces produces thrilling blood interaction candidates. Many work continues in production of PVPmodified materials, including surgical devices, for use in biomedical applications. Better PVP immobilization techniques are necessary for a variety including substrates, rubber, metal etc. The relationship between blood, tissues and modified surfaces of PVP must be explained and understood. As most bio interaction experiments have been performed in vitro to date, a particular requirement is required for in vivo testing. In addition, the scope of these tests should be expanded to include NVP copolymers, especially ring copolymers.

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#### REFERENCES

- Q. Yu, Y. Zhang, H. Chen, F. Zhou, Z. Wu, H. Huang, J. L. Brash, Langmuir, 2010, 26, 8582.
- Q. Yu, Y. Zhang, H. Chen, Z. Wu, H. Huang, C. Cheng, Colloids Surf., B. 2010, 76, 468.
- L. Yuan, H. Wang, Q. Yu, Z. Wu, J. L. Brash, H. Chen, J. Mater. Chem. 2011, 21, 6148.
- H. Wang, L. Wang, P. Zhang, L. Yuan, Q. Yu, H. Chen, Colloids Surf., B. 2011, 83, 355.
- Q. Yu, X. Li, Y. Zhang, L. Yuan, T. Zhao, H. Chen, RSC Advances, 2011, 1, 262.
- L. Wang, H. Wang, L. Yuan, W. Yang, Z. Wu, H. Chen, J. Mater. Chem. 2011, 21, 13920.
- D. Neugebauer, K. Matyjaszewski, Macromolecules, 2003, 36, 2598.
- A. Debuigne, N. Willet, R. Je'ro<sup>^</sup>me, C. Detrembleur, Macromolecules, 2007, 40, 7111.
- X. Lu, S. Gong, L. Meng, C. Li, S. Yang, L. Zhang, Polymer, 2007, 48, 2835.
- 10. W. He, K. E. Gonsalves, J. H. Pickett, C. Halberstadt, Biomacromolecules, 2003, 4, 75.
- 11. W. He, C. R. Halberstadt, K. E. Gonsalves, Biomaterials 2004, 25, 2055.
- M.-Y. Ahn, I.-T. Hwang, C.-H. Jung, Y.-C. Nho, J.-H. Choi, K. M. Huh, J. Ind. Eng. Chem. 2010, 16, 87.
- C.-H. Choi, S. H. Hagvall, B. M. Wu, J. C. Y. Dunn, R. E. Beygui, C.-J. Kim, Biomaterials, 2007, 28, 1672.
- X. Xu, C. Zhang, Y. Zhou, Q. Liu, J. Cheng, K. Yao, Q. Chen, J. Bioact. Compat. Polym. 2007, 22, 195.

- Z. Wu, H. Chen, X. Liu, Y. Zhang, D. Li, H. Huang, Langmuir, 2009, 25, 2900.
- T. E. Andersen, Y. Palarasah, M.-O. Skjødt, R. Ogaki, M. Benter, M. Alei, H. J. Kolmos, C. Koch, P. Kingshott, Biomaterials, 2011, 32, 4481.
- F. Bre'tagnol, M. Lejeune, A. Papadopoulou-Bouraoui, M. Hasiwa, H. Rauscher, G. Ceccone, P. Colpo, F. Rossi, Acta Biomater. 2006, 2, 165.
- H. Chen, C. Peng, Y. Yao, J. Wang, Z. Chen, Z. Yang, L. Xia, S. Liu, J. Appl. Polym. Sci. 2009, 114, 3152.
- M. Matsuda, K-i. Yamamoto, T. Yakushiji, M. Fukuda, T. Miyasaka, K. Sakai, J. Membr. Sci. 2008, 310, 219.
- M. Hayama, K-i. Yamamoto, F. Kohori, T. Uesaka, Y. Ueno, H. Sugaya, I. Itagaki, K. Sakai, Biomaterials, 2004, 25, 1019.
- N. Nady, M. C. R. Franssen, H. Zuilhof, M. S. M. Eldin, R. Boom, K. Schro"en, Desalination, 2011, 275, 1.
- X. Liu, K. Sun, Z. Wu, J. Lu, B. Song, W. Tong, X. Shi, H. Chen, Langmuir, 2012, 28, 9451.
- Z. Jin, W. Feng, S. Zhu, H. Sheardown, J. L. Brash, J. Biomater. Sci. Polymer Edn. 2010, 21, 1331.
- S. L. McArthur, K. M. McLean, P. Kingshott, H. A. W. St John, R. C. Chatelier, H. J. Griesser, Colloids Surf., B. 2000, 17, 37.
- 25. B. Gao, H. Hu, J. Guo, Y. Li, Colloids Surf., B. 2010, 77, 206.
- D. Wang, D. J. T. Hill, F. Rasoul, A. K. Whittaker, Radiat. Phys. Chem. 2011, 80, 207.
- K. Reimer, P. M. Vogt, B. Broegmann, J. Hauser, O. Rossbach, A. Kramer, P. Rudolph, B. Bosse, H. Schreier, W. Fleischer, Dermatology 2000, 201, 235.
- M. Ignatova, O. Stoilova, N. Manolova, N. Markova, I. Rashkov, Macromol. Biosci. 2010, 10, 944.
- 29. P. A. Williams, Handbook of Industrial Water Soluble Polymers, Blackwell Publishing Ltd, 2008.
- A. T. Florence, D. Attwood, Physicochemical principles of pharmacy, Pharmaceutical Press, London, 2006.
- 31. V. Buhler, Polyvinylpyrrolidone Excipients for Pharmaceuticals, Springer, Berlin Heidelberg, 2005.

- 32. xiaoli Liu, Yajun Xu, Zhaoqiang Wu, Hong Chen. Poly (Nvinylpyrrolidone)-modified surfaces for biomedical applications. Macromol. Biosci, 2013, 13, 147-154
- 70 Jahre Polyvinylpyrrolidon Zu Ehren von Prof. Dr. Walter Reppe FRANK FISCHER | STEPHAN BAUERChem. Unserer Zeit, 2009, 43, 376 – 383.
- H. Chen, M. A. Brook, Y. Chen, H. Sheardown, J. Biomater. Sci. Polymer Edn 2005, 16, 531.
- 35. H. Chen, Z. Zhang, Y. Chen, M. A. Brook, H. Sheardown, Biomaterials 2005, 26, 2391.